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TEST-RETEST RELIABILITY OF OXFORD MEDILOG 9000 SLEEP RECORDING AND SS-90-III SLEEP STAGE SCORING

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REPORT NO. 89-6

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Test-Retest Reliability of Oxford Medilog 9000
Sleep Recording and SS-90-III Sleep Stage Scoring

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A-1	

Report No. 89-6, supported by the Naval Medical Research and Development Command, Bethesda, MD, Department of the Navy, under Work Unit MR4101-003-.6003. This research was conducted during the author's first appointment as an ASEE Summer Faculty Fellow, 1988. The opinions expressed in this paper are those of the authors and do not reflect official policy or position of the Navy, Department of Defense, not the U. S. Government. The authors wish to acknowledge the valuable assistance of Neal Morrison and Larry Matteson in the statistical analysis of the data, and Gary Welton who provided the method for the analysis of reliability of the data. Laverne Johnson, Steven A. Gomez, and Cheryl L. Spinweber also made important suggestions at various phases in this project.

SUMMARY

This study was undertaken to assess the test-retest reliability of the expanded Medilog SS-90-III Sleep Stager by comparing sleep stager scoring of the same records scored more than once. Subjects consisted of 19 normal sleepers who slept one night at home, following their normal routine. They ranged in age from 19.3 to 63.5, with mean = 31.1 and median = 24.7. There were 15 males and 4 females.

All sleep tapes were processed five consecutive times on the day of sleep scoring, termed runs 1-5. Dependent variables chosen for study consisted of: total sleep period, actual sleep time, wake after sleep onset (greater and less than 120 sec.), total movement time, total stage 1, total stage 2, total stage 3, total stage 4, total REM, percent of stage 1, percent of stage 2, percent of stage 3, percent of stage 4, percent of stage REM, start to sleep onset, sleep onset to REM, sleep onset to stage 2, sleep onset to stage 3, and sleep onset to stage 4.

Pearson correlations and alpha coefficients were calculated to evaluate the reliability of each measure over the five runs combined. Correlations between runs ranged between .878 and 1.00 for all measures, except sleep onset to REM through sleep onset to stage 4, where correlations ranged from -.003 to .991. Alpha coefficients ranged from .98 to 1.00 for all measures, including total sleep time, movement time, sleep onset, waking after sleep onset, and both absolute and percentage amounts of sleep stages 1-4 and REM, but not including the latency measures. Alpha coefficients for the latency measures were less reliable, although acceptable for REM latency, marginally so for stage 2 and 3 latencies, but not acceptable for stage 4 latency.

INTRODUCTION

Important technical advances in portable sleep recording and automated EEG sleep stage scoring methods have been introduced in recent years. These improved methods offer several economies for both subjects and investigators by virtue of the fact that sleep data are recorded on portable cassette tape EEG recorders. The recording electrodes can be applied almost any time day or night at the technologist's convenience, and the portability of the equipment means that subjects can choose to sleep at home, or in other, more familiar, environments. Further, the cassette tape can be scored in as little as 30-60 minutes and stored indefinitely as needed at minimal cost and space. Thus, this improved procedure has important advantages for (1) improved subject acceptance leading potentially to better sleep, (2) a more flexible workload for the technologist, and (3) quicker, yet reliable scoring of sleep records.

Evaluative reports in the literature have generally confirmed these advantages. Sewitch and Kupfer (1,2) have reported a project in which they compared the Oxford Medilog 9000 and Telediagnostic systems with laboratory recordings. They concluded that there were no differences in standard EEG sleep parameters recorded in either the home or laboratory. Hoelscher et al. (3) studied the usefulness of the Oxford Medilog system in evaluating a variety of sleep/wake disorders in a large clinical population and concluded that "the Oxford-Medilog 9000 can be used to evaluate a variety of sleep-related disorders, results in acceptable recordings in 90-97% of all studies, and is well-accepted by most patients" (p.607). However, both Sewitch and Kupfer and Hoelscher et al. noted difficulties in some cases, as well as remaining questions in scoring details.

More recently, Crawford (4) and Holler and Riemer (5) both compared visually-scored versus Medilog Sleep Stager-scored sleep records, in an effort to assess the accuracy and reliability of the automated method. Crawford found a range of 74 to 89% agreement (mean = 84% epoch by epoch) between manual and automated sleep scoring of 20 recordings. However, Holler and Riemer found consistent differences in (1) sleep onset time and (2) REM time, but not any other sleep measures, between manual and automated methods when applied to their sample of four sleep records. Neither Crawford nor Holler and Riemer compared automated sleep stager scoring of the same records scored more than once, i.e., correlation of the automated method with itself.

Further, while the reports of these investigators do indicate an acceptable level of reliability of automated sleep scoring by the Medilog Sleep Stager, it should be noted that the software supporting this system has been recently revised and expanded, thus requiring a revised and expanded evaluation of the scoring. The present study was therefore undertaken to evaluate the reliability of the expanded Medilog SS-90-III Sleep Stager by comparing sleep stager scoring of the same records scored more than once.

METHODS

Subjects

Subjects consisted of 21 healthy, normal sleepers recruited in the San Diego area. Four subject-night recordings were rejected because of electrode failure or inability of the subject to sleep more than four hours. Two of these were successfully rescheduled for a second night, and two were dropped from the study.

Therefore, the final N consisted of 19 subjects, ranging in age from 19.3 to 63.5 years, with mean = 31.1 and median = 24.7 years. There were 15 males and 4 females. Mean age of the females was not significantly different from the males (means of 32.7 and 30.9 years, respectively).

Procedures

Electrode attachment for most subjects was scheduled between 1400-1600 at the sleep laboratory, although in a minority of cases this was done at the subject's work location. Subjects then slept at home, following their normal routine, and returned to the laboratory about 0600-0700 for removal of the electrodes. Several subjects were given a bottle of acetone to remove the electrodes by themselves at home in the morning.

The standard sleep-monitoring montage consisted of the following: one channel of EEG (C4 to opposite mastoid), two channels of EOG (outer canthus to opposite mastoid), and one channel of EMG from the submental muscle of the chin. Clock time was used to define the beginning and end of the total sleep period (TSP).

Sleep scoring of all tapes was conducted 1-2 days after the recording night. All recommended procedures in the 1987 operator's manuals (Medilog 9000 Replay and Display System Operator's Instruction and Service Manual; Medilog SS-90-III Sleep Stager Operator's Manual) supplied by Oxford Medical Ltd. were followed closely. All tapes were processed on the Sleep Stager five consecutive times on the day of sleep scoring (i.e., five independent

scoring runs always conducted on the same day), hereafter referred to as runs 1-5.

The Sleep Stager provides a printout with a hypnogram (see sample in Crawford (4)), plus the following measures: total sleep period (TSP), actual sleep time (AST), wake after sleep onset (WASO) > 120 sec., wake after sleep onset (WASO) < 120 sec., total movement time (TMT), total stage 1 (TOT1), total stage 2 (TOT2), total stage 3 (TOT3), total stage 4 (TOT4), total REM (TOTR), start to sleep onset (SSO), sleep onset to first REM (SOR), sleep onset to stage 2 (S02), sleep onset to stage 3 (S03), sleep onset to stage 4 (S04).

Of this list, all measures from AST to TOTR were provided in more than one unit of measurement or format, viz., by (1) number of epochs (30 secs.), (2) number of episodes (any occurrence lasting one epoch or more), (3) number of minutes, (4) percent of total sleep period, and (5) percent of actual sleep time (where appropriate). Thus, because of duplication, it was necessary to choose a smaller yet representative group of dependent variables for the present study. This group is listed in Table 1. All time measures are given in minutes. Latencies are calculated to the first four contiguous epochs (2 min.) of the stage. There is a partial duplication of measures only in that sleep stages 1 through REM are listed by both total time (TOT1-TOTR) and percent of actual time (PER1-PERR).

RESULTS

Means, standard deviations, and minimum and maximum values for all measures and all runs are summarized in Table 1. The minimum values listed are the lowest of the five minima of five runs, and the maximum values are the highest of the five maxima of five runs.

Pearson correlations between runs

Pearson correlation coefficients were calculated between consecutive sleep stage runs, which produced five correlation coefficients for each dependent variable. Runs were paired as follows: 1-2, 2-3, 3-4, 4-5, and 5-1. The range of these correlations between runs for each dependent variable is given in Table 1. It can be seen that the correlations between runs for the first 16 variables (TSP to SSO) were always between .878 and 1.00. Twenty-nine out of 32 correlations were .90 or above, and the remaining three were above .87. For the four latency measures, SOR to S04, the range of

Table 1: Summary of mean, standard deviation, minimum and maximum value, range of Pearson correlations between runs, and alpha reliability coefficient for each of the dependent measures, all runs (1-5) combined.

MEASURE	MEAN	STD DEV	MIN	MAX	RANGE OF CORRELATIONS BETW RUNS	ALPHA COEFF
TSP	476.11	81.28	330.0	653.5	.998-1.00	1.000
AST	400.44	71.32	265.0	542.0	.972-.999	.998
WASOG	89.83	71.89	0.0	265.0	.945-.994	.994
WASOL	58.75	29.85	5.0	132.0	.899-.987	.989
TMT	2.75	4.93	0.0	18.0	.962-.990	.996
TOT1	119.90	119.74	2.0	422.0	.977-.994	.997
TOT2	261.46	132.40	0.0	460.0	.878-.997	.989
TOT3	41.41	35.12	0.0	131.0	.993-.997	.999
TOT4	49.14	60.99	0.0	215.0	.997-1.00	1.000
TOTR	328.91	155.24	59.0	677.0	.969-.998	.997
PER1	15.49	15.48	0.2	57.8	.976-.994	.997
PER2	32.30	15.17	0.0	54.8	.877-.997	.988
PER3	5.01	4.05	0.0	13.4	.990-.998	.999
PER4	5.79	6.90	0.0	19.9	.996-.999	1.000
PERR	41.39	17.86	6.4	82.9	.970-.997	.997
SSO	15.63	15.94	0.0	72.5	.944-.994	.994
SOR	56.64	58.57	0.0	432.5	.779-.971	.943
S02	24.01	46.87	0.0	408.5	.097-.824	.645
S03	41.49	78.82	0.0	438.0	.243-.830	.761
S04	16.13	36.63	0.0	497.0	-.003-.991	.246

NOTE: N = 19; r of .43 = $p < .05$; r of .55 = $p < .01$. Abbreviations: TSP = total sleep period, AST = actual sleep time, WASOG = waso > 120 sec., WASOL = waso < 120 sec, TMT = total movement time TOT1 = total stage 1, TOT2 = total stage 2, TOT3 = total stage 3, TOT4 = total stage 4, TOTR = total REM, PER1 = % stage 1, PER2 = percent stage 2, PER3 = percent stage 3, PER4 = percent stage 4, PERR = percent stage REM, SSO = start to sleep onset, SOR = sleep onset to REM, S02 = sleep onset to stage 2, S03 = sleep onset to stage 3, S04 = sleep onset to stage 4.

Pearson correlations were from -.003 to .991, and all of the three minimum correlations listed between runs for these measures failed to reach statistical significance at $p < .05$.

Alpha reliability coefficients

Alpha coefficients, using a method described by Cronbach (6), were calculated in order to evaluate the reliability of each measure over the five runs combined, based on the ratio of the variance of each individual measure to the variance of the composite of the five runs. The resulting alpha coefficients are given in Table 1. It can be seen that the alpha coefficients for the first 126 measures, TSP to SS0, are consistently .98 to 1.00, indicating very high reliability. For the latency measures (SOR to S04), however, the alpha coefficients decline from .94 to .24, respectively, the latter failing to reach statistical significance in the case of S04. While the alpha coefficients for S04, S02, and S03 were significant at $p < .01$, one might still question whether the correlations of .64 and .76 for S02 and S03, respectively, are acceptable reliabilities for an automated scoring procedure.

DISCUSSION

The primary findings of this study may be summarized as follows: (1) Medilog SS-90-III Sleep Stager scoring of most sleep measures was highly reliable, with alpha coefficients ranging from .98 to 1.00 for measures including total sleep time, movement time, sleep onset, waking after sleep onset, and both absolute and percentage amounts of sleep stages 1-4 and REM; (2) scoring of latency measures was less reliable, although certainly acceptable for REM latency (SOR), and marginally acceptable for stage 2 and 3 latencies (S02 and S03), but not acceptable for an automated scoring of stage 4 latency (S04).

While direct comparison with previous reports is difficult due to differences in procedures and methods of analysis, it would appear that our findings with the Medilog SS-90-III Sleep Stager represent a very considerable improvement over the results reported by both Crawford (4) and Holler and Riemer (5). Crawford found an average 74% agreement between manual and machine scoring across epochs for all measures, clearly suggesting a lower reliability, although she was not assessing retest reliability. Similarly, Holler and Riemer reported consistent error in measures of sleep onset and REM time, although neither of these variables appeared as problems in our data. While we did not compare manual and automated scoring provides a benchmark of retest reliability to which the manual method can only aspire.

Clear exceptions to this statement were the latency measures, S02, S03, and S04 - especially the latter - where alpha coefficients were either

marginally or unacceptably low. Reasons for this difficulty are undoubtedly that the stager defined latencies as the first four contiguous epochs of a given stage. Thus, for example, in measuring stage 4 onset, the scoring sequence 3444434443 would count, whereas 3444334443 would not, even though the overall accuracy of scoring was consistently high. Whenever the sleep stager missed the onset of a stage in this manner, and the subject did not show that stage again at all or until much later, then the latency value was greatly increased. Clearly, this effect would be larger in the case of a sleep stage that occurred most frequently, as was true of stage 4 sleep. Of the total of 285 reports of latency to onset sleep stages 2, 3, and 4, such shifts were observed in 10 cases, or 3.5%. Of this 10, three involved stage 2, three involved stage 3, and four involved stage 4.

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Unclassified

SECURITY CLASSIFICATION OF THIS PAGE

REPORT DOCUMENTATION PAGE

1a REPORT SECURITY CLASSIFICATION Unclassified			1b RESTRICTIVE MARKINGS N/A	
2a SECURITY CLASSIFICATION AUTHORITY N/A			3 DISTRIBUTION/AVAILABILITY OF REPORT Approved for public release; distribution unlimited.	
2b DECLASSIFICATION/DOWNGRADING SCHEDULE N/A				
4. PERFORMING ORGANIZATION REPORT NUMBER(S) NHRC Report No. 89-6			5 MONITORING ORGANIZATION REPORT NUMBER(S)	
6a NAME OF PERFORMING ORGANIZATION Naval Health Research Center		6b OFFICE SYMBOL (If applicable) 50	7a NAME OF MONITORING ORGANIZATION Commander Naval Medical Command	
6c ADDRESS (City, State, and ZIP Code) P. O. Box 85122 San Diego, CA 92138-9174			7b ADDRESS (City, State, and ZIP Code) Department of the Navy Washington DC 20371	
8a NAME OF FUNDING/SPONSORING ORGANIZATION Naval Medical Research & Development Command		8b OFFICE SYMBOL (If applicable)	9. PROCUREMENT INSTRUMENT IDENTIFICATION NUMBER	
8c ADDRESS (City, State, and ZIP Code) Naval Medical Command National Capital Region Bethesda, MD 20814-5044			10. SOURCE OF FUNDING NUMBERS	
			PROGRAM ELEMENT NO. 61155N	TASK NO. MR4101
			TASK NO. 003	WORK UNIT ACCESSION NO. 6003
11 TITLE (Include Security Classification) (U) TEST-RETEST RELIABILITY OF OXFORD MEDILOG 9000 SLEEP RECORDING AND SS-90-III SLEEP STAGE SCORING				
12 PERSONAL AUTHOR(S) DAVID G. MCDONALD AND LORENE IRWIN				
13a TYPE OF REPORT Interim		13b TIME COVERED FROM _____ TO _____	14. DATE OF REPORT (Year, Month, Day) 1989March13	
15 PAGE COUNT				
16 SUPPLEMENTARY NOTATION Prepared in cooperation with the University of Missouri-Columbia during an appointment of the senior author as an ASEE Summer Faculty Fellow, 1988.				
17 COSATI CODES			18 SUBJECT TERMS (Continue on reverse if necessary and identify by block number) Medilog system; Sleep scoring; EEG sleep; Portable recordings; Normal sleepers	
FIELD	GROUP	SUB-GROUP		
19 ABSTRACT (Continue on reverse if necessary and identify by block number) Sleep was recorded in 19 normal sleepers (19.3-63.5 years of age) one night at home, using the Medilog 9000 system to assess the reliability of the Medilog SS-90-III Sleep Stager by comparing sleep stager scoring of the same records scored five times. Primary results were: (1) Sleep Stager scoring of most sleep measures was highly reliable, with alpha coefficients ranging from .98 to 1.00 for total sleep time, movement time, sleep onset, waking after sleep onset, and both absolute and percentage amounts of sleep stages 1-4 and REM; (2) scoring of latency measures was less reliable, although certainly acceptable for REM latency and marginally acceptable for stage 2 and 3 latencies, but not acceptable for an automated scoring of stage 4 latency.				
20 DISTRIBUTION/AVAILABILITY OF ABSTRACT <input checked="" type="checkbox"/> UNCLASSIFIED/UNLIMITED <input checked="" type="checkbox"/> SAME AS RPT <input type="checkbox"/> DTIC USERS			21. ABSTRACT SECURITY CLASSIFICATION Unclassified	
22a NAME OF RESPONSIBLE INDIVIDUAL David McDonald, Ph.D./Lorene Irwin			22b TELEPHONE (Include Area Code) (619) 532-6114	22c. OFFICE SYMBOL 50